

Human acid-insoluble dentin with BMP-2 accelerates bone induction in subcutaneous and intramuscular tissues

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Dentin matrix is well known as the most insoluble collagen in human body. We already confirmed the osteoinductive property by granules of human demineralized dentin matrix (DDM) histologically. Human DDM granules and human demineralized root-dentin (DRD) mass were prepared from adult vital teeth. The hard tissue induction by DDM alone or DRD alone was estimated at 4 weeks after implantation. The DDM alone induced bone and cartilage independently. In addition, the bioassay by recombinant human BMP-2 (5.0 µg)/DDM or BMP-2 (5.0 µg)/DRD was estimated in mouse subcutaneous or intramuscular tissues, respectively. Histological examination showed that the BMP-2/DDM induced bone and marrow, and the DDM granules were partially absorbed by new bone. The morphometric analysis demonstrated that the BMP-2/DDM showed 36.3% in the volume of bone and marrow, while the DDM alone showed 1.3% at 4 weeks. Moreover, the BMP-2/DRD also induced active bone formation on the root surface and in the pulp cavity. These results indicate that BMP-2 significantly accelerated bone formation in decalcified dentin implants. Human recycled DDM and DRD might be effective materials as osteoinductive collagenous carriers of BMP-2 for bone engineering.

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1. Introduction

Dentin is an acellular collagen-rich tissue matrix without vessels, while bone is a cellular tissue with vessels. However, dentin and bone have similar components that consist of 10% body fluid, 20% organic materials, and 70% minerals as mainly hydroxyapatite (HAp), and contain bone morphogenetic proteins (BMPs) with inducing capability of bone and cartilage in non-skeletal sites.¹⁾ Recombinant human BMP-2, 4, and 7 are strong accelerating factors of bone induction,^{2,3)} and BMP-2 and 7 are available for clinical use in USA and European Union.

The bone-inducing property of dentin was discovered in 1967 that rabbit demineralized dentin matrix (DDM) induced bone in the intramuscular tissues.⁴⁾ There are several *in vivo* studies that the animal DDM induced ectopic bone formation in subcutaneous and intramuscular pockets in rodents.^{5,6)} We confirmed histologically that human completely demineralized dentin granules induced bone and cartilage independently in nude mice.^{7,8)} On the other hand, human partially demineralized dentin granules failed to induce bone formation in the intramuscular pockets.⁹⁾ These reports indicated that dentin preparation such as shape and acid-treatment conditions was critical for bone-inducing property of dentin. Though DDM and DRD are defined as acid-insoluble collagen binding natural BMPs, we considered human recycled DDM and DRD as absorbable biomaterials for the better performances of recombinant human BMP-2.

The purpose of this study is to estimate the efficacy of the granule type and the root type of human completely demineralized dentin as carrier matrices for the BMP-2 delivery system.

2. Experimental procedure

2.1 Experiment 1

2.1.1 Preparation of dentin granules

The human, adult third molar teeth were crushed under the ice cooling, using our developed auto-mill with ZrO₂ vessel and blade (Figs. 1, 2), and completely demineralized in 2% HNO₃ solution (pH 1.0) for DDM (Figs. 1-3). The acid-insoluble DDM granules were sieved (size: 0.5-1.0 mm), lyophilized and reserved in -80°C before use. The insoluble dentin collagen is not expanded in HCl solution (pH 2.0), while the expansion rates of skin collagen and bone collagen are about 4.0 and 1.2 times, respectively.¹⁰⁾

2.1.2 Addition of BMP-2 solution

One hundred micro-liter of recombinant human BMP-2 (50 µg/ml PBS) solution was added by pipetting to 70 mg of DDM in a cut-opened tuberculin syringe (1 ml, TERUMO[®]) just before the operations. Recombinant human BMP-2 was supplied by Astellas Pharma Inc. (Tokyo, Japan), and was prepared at a concentration of 0.1 µg of BMP-2 per microliter of phosphate buffered saline (PBS).

2.1.3 Bioassay

Nude mice (male, 4 week-old), deficient in immunogenic reactions, were subjected to intraperitoneal anesthesia with pentobarbital sodium (4 mg/100 g body weight). BMP-2 (5.0 µg)/DDM (70 mg) were implanted into the subcutaneous

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Fig. 1. Extracted tooth with 20 ices in ZrO₂ vessel before crushing.

Fig. 2. Automatic mill. Newly developed mill (Patents: International application No. PCT/JP2007/053321, International published No. WO2007/099861 A1).

tissues in back. The incisions were sutured with nylon threads. The implanted materials were removed at 4 weeks after the operations. All procedures were followed the Guidelines in Health Sciences University of Hokkaido for Experiments on Animals.

2.1.4 Histomorphological examinations

The explanted samples were fixed in 10% neutral buffered formalin for 3 days, decalcified with decalcified for 7 days with 10% formic acid and embedded in paraffin. Decalcified sections (4 µm in thickness) were made and stained with hematoxylin and eosin (HE). For morphometric analysis, tissues of the specimens were divided into five compartments: bone, cartilage, marrow, dentin matrix (DDM), and connective tissue. The compartments were measured by using Weibel method^[11] at 3 separate points, 100 µm apart, the midpoint being at center of the implant. The average value of these 3 points was used as the mean area of each implant.

2.2 Experiment 2

2.2.1 Preparation of root-dentin

Crowns were cut from human teeth and roots were collected. The roots were completely decalcified in 2% HNO₃ solution (pH 1.0) for demineralized root-dentin (DRD). The acid-insoluble DRD were lyophilized and reserved in -80°C before use.

2.2.2 Addition of BMP-2 solution

One hundred micro-liter of recombinant human BMP-2 (50 µg/ml PBS) solution was added by pipetting to DRD in a sterilized tube just before the operations.

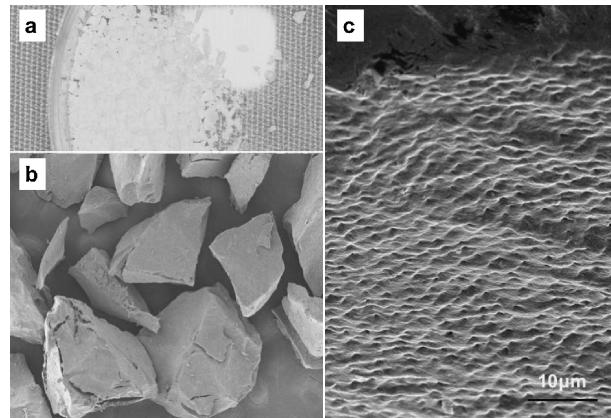


Fig. 3. Aspects of DDM granules. a. freeze-dried DDM before graft, b. SEM of DDM, c. higher magnification of b. Note: Dentinal tubes.

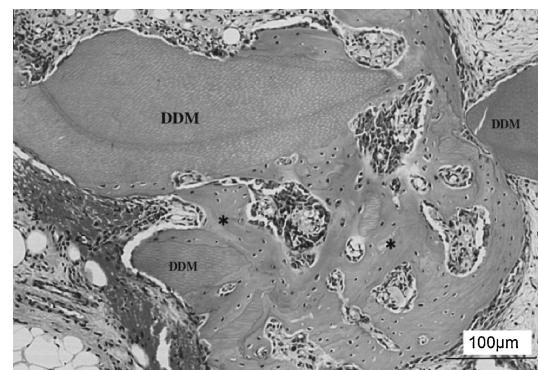


Fig. 4. Histological photograph of decalcified section of BMP-2/DDM at 4 weeks. * induced bone (HE).

2.2.3 Bioassay

BMP-2 (5.0 µg)/DRD were implanted into the hindquarter muscles in the nude mice (male, 4 week-old). At 4 weeks after the operations, the legs including implants were amputated and fixed with 10% neutral buffered formalin, decalcified for 10 days with 10% formic acid and embedded in paraffin. Decalcified sections (4 µm in thickness) were made and stained with hematoxylin and eosin (HE). All procedures were followed the Guidelines in Aichi-Gakuin University for Experiments on Animals.

2.2.4 Radiography and histological examinations

The samples were photographed by X-ray machine (25 mA, 24 s), and then fixed in 10% neutral buffered formalin, decalcified with 10% formic acid, embedded in paraffin, sectioned and stained with HE.

3. Results

3.1 Experiment 1

3.1.1 Histological findings

In the BMP-2/DDM, osteoblast differentiation occurred on the surface of DDM, while chondroblast differentiation was not observed at 4 weeks (Fig. 4). Giant cells appeared on DDM surface and the absorption of DDM proceeded from the surfaces (Fig. 5). In DDM alone, new bone was found on the surface of DDM, and cartilage was observed at 4 weeks between DDM granules.

3.1.2 Histomorphometrical analysis

The morphometric results are shown in Table 1. The BMP-2/

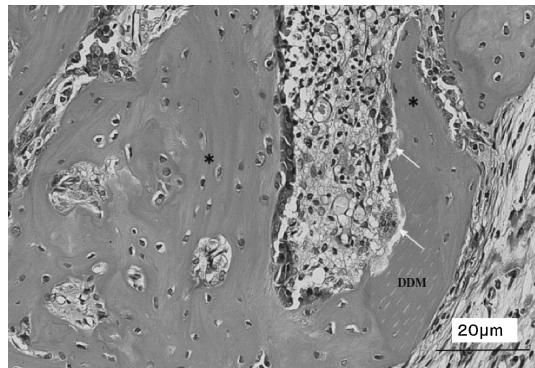


Fig. 5. Histological photograph of decalcified section of BMP-2/DDM at 4 weeks. ↑ giant cell on DDM. * Induced bone (HE).

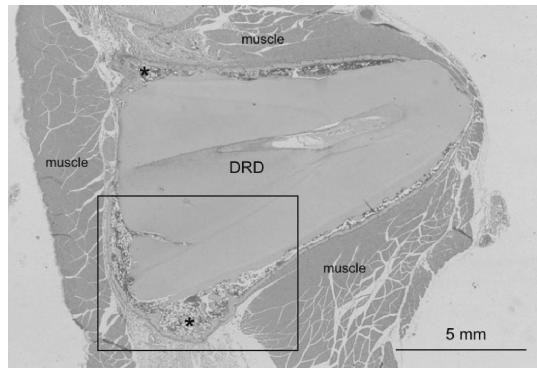


Fig. 7. Histological photograph of decalcified section of BMP-2/DRD at 4 weeks. * Bone marrow on decalcified root (HE).

Table 1. Morphometric analysis (%)

Implant	Bone	Cartilage	Marrow	DDM	Connective tissue
DDM alone	0.9 ± 0.1	0.4 ± 0.2	0.4 ± 0.1	74.7 ± 4.9	23.6 ± 5.0
DDM/BMP-2	28.3 ± 2.6	0	8.0 ± 2.9	34.4 ± 2.9	29.3 ± 2.1

All tissues: 100%, Value: mean ± SD

Number: 3–9 implants, Explanted time: 4 weeks

DDM implant showed 36.3% at 4 weeks in the total volume of bone and marrow, while the DDM alone implant showed 1.3%. The BMP-2/DDM showed 0.0% in cartilage, while the DDM alone implant showed 0.4%. The ratio of DDM residues in the BMP-2/DDM was 67.5% of that in the DDM alone.

3.2 Experiment 2

3.2.1 X-ray findings

In the BMP-2/DRD, bone-like radiopaque was observed around DRD, while calcified tissues were not found in the DRD alone (Fig. 6).

3.2.2 Histological findings

In the BMP-2/DRD, active bone formation was observed around DRD and in micro-cracks at 4 weeks (Fig. 7). Mesenchymal cells invaded into the micro-cracks and pulp spaces. DRD mass was incorporated by trabecular bone and marrow (Fig. 8). Giant cells phagocytized DRD matrix, partially. In the DRD alone, bone and cartilage were not observed.

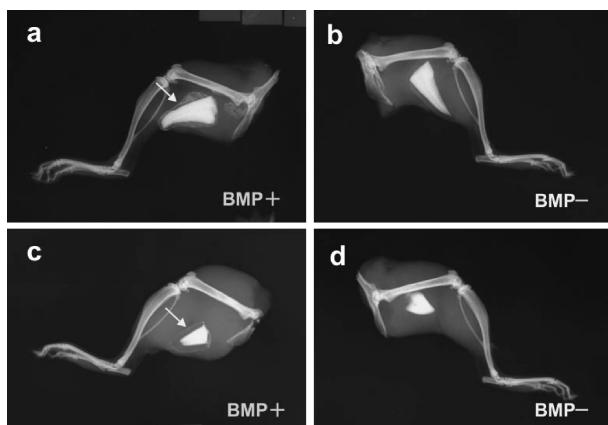


Fig. 6. Radiograph of intramuscular implants of BMP-2/DRD and DRD alone at 4 weeks. a, c: BMP-2/DRD, ↑ hard tissue-like radiopacity; b, d: DRD alone; a, b: same mouse; c, d: same mouse.

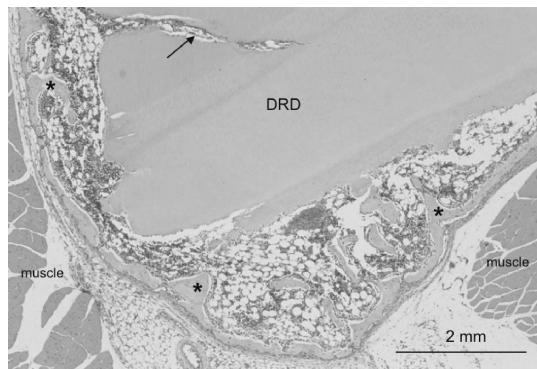


Fig. 8. Higher magnification of □ in Fig. 7. * bone trabeculae, ↑ cervical crack.

4. Discussion

Bone morphogenetic proteins (BMPs) are strong accelerating factors with bone-inducing activity.^{1),3)} Dentin-derived BMPs were extracted with 4 M guanidine HCl, and partially purified from rat, rabbit, and bovine.^{12)–15)} The demineralized treatment for bone and dentin increase their osteoinductivity and decrease their antigenicity.¹⁶⁾ Even after demineralization, active types of BMPs bind collagen-rich matrices.¹⁷⁾ The decalcified dentin is more absorbable, bone-inducing matrix than the calcified dentin,⁴⁾ and roll type of decalcified dentin membrane revealed better activity of bone induction.¹⁸⁾ Considering these reports, we believe that HA crystals inhibit release of growth factors as natural BMPs and resist enzyme digestion of dentin collagen, and that the added BMP-2 binds demineralized dentin (DDM, DRD) with both chemical ion-bond and physical adsorption, while natural BMPs binds collagen with covalent bond. In the present study, histological examination showed that the BMP-2/DDM implant and the BMP-2/DRD implant induced bone and marrow, and that DDM granules and DRD mass were partially absorbed (Figs. 4, 6). In the BMP-2/DDM, interconnected bone formation occurred between DDM granules (Fig. 4). On the other hand, in the BMP-2/DRD, bone and marrow were found on the root surface, in the pulp cavity, and in the cracks (Fig. 6). In previous studies, the DDM alone induced bone and cartilage independently, while the DRD alone did not induce bone and cartilage in the mice model at 4 weeks.^{8),9)} The morphometric analyses demonstrated that the BMP-2/DDM showed 36.3% in the volume of bone and marrow and 0% in the volume of cartilage, while the DDM alone showed 1.3% and 0.4%, respectively at 4 weeks (Table 1). These results indicated that BMP-2 accelerated

osteoinduction in the granular implant system of DDM. We believe that the granule type and the root type of human dentin will be effective as collagenous carriers of BMP-2 for bone regeneration. Dentin is an acellular collagen-rich tissue, which has bone-inducing and bioabsorbable properties. Especially, autologous dentin has the potential advantages of cell adhesion domain sequences (RGD) and biological recognition. The use of autologous tissues avoids the immune-rejection, and the deleterious side effects of immunosuppressive medications. The autologous dentin collagen is superior to animal-derived materials as medical use. Therefore, human dentin will be able to be recycled in auto-transplantation similar to bone autograft for bone regeneration.

5. Conclusions

BMP-2 significantly accelerated bone formation in granular and root type carriers of human decalcified dentin. We concluded that human recycled DDM and DRD might be effective biomaterials as carriers of BMP-2 for autologous bone engineering.

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